

# Modeling Gain and Gradedness of $\text{Ca}^{2+}$ Release in the Functional Unit of the Cardiac Diadic Space

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**ABSTRACT** A model of the functional release unit (FRU) in rat cardiac muscle consisting of one dihydropyridine receptor (DHPR) and eight ryanodine receptor (RyR) channels, and the volume surrounding them, is formulated. It is assumed that no spatial  $[\text{Ca}^{2+}]$  gradients exist in this volume, and that each FRU acts independently. The model is amenable to systematic parameter studies in which FRU dynamics are simulated at the channel level using Monte Carlo methods with  $\text{Ca}^{2+}$  concentrations simulated by numerical integration of a coupled system of differential equations. Using stochastic methods,  $\text{Ca}^{2+}$ -induced  $\text{Ca}^{2+}$  release (CICR) shows both high gain and graded  $\text{Ca}^{2+}$  release that is robust when parameters are varied. For a single DHPR opening, the resulting RyR  $\text{Ca}^{2+}$  release flux is insensitive to the DHPR open duration, and is determined principally by local sarcoplasmic reticulum (SR)  $\text{Ca}^{2+}$  load, consistent with experimental data on  $\text{Ca}^{2+}$  sparks. In addition, single RyR openings are effective in triggering  $\text{Ca}^{2+}$  release from adjacent RyRs only when open duration is long and SR  $\text{Ca}^{2+}$  load is high. This indicates relatively low coupling between RyRs, and suggests a mechanism that limits the regenerative spread of RyR openings. The results also suggest that adaptation plays an important modulatory role in shaping  $\text{Ca}^{2+}$  release duration and magnitude, but is not solely responsible for terminating  $\text{Ca}^{2+}$  release. Results obtained with the stochastic model suggest that high gain and gradedness can occur by the recruitment of independent FRUs without requiring spatial  $[\text{Ca}^{2+}]$  gradients within a functional unit or cross-coupling between adjacent functional units.

## INTRODUCTION

Calcium-induced calcium release (CICR) in cardiac muscle exhibits both gradedness and high gain. Gradedness refers to the observation that sarcoplasmic reticulum (SR)  $\text{Ca}^{2+}$  release is proportional to the influx of trigger  $\text{Ca}^{2+}$  (Beuckelmann and Wier, 1988), whereas high gain refers to the observation that  $\text{Ca}^{2+}$  release from SR is significantly larger than the trigger influx (Fabiato, 1985a). The paradox, as described by Stern (1992) is that the positive feedback inherent in such high-gain systems produces all-or-none rather than graded  $\text{Ca}^{2+}$  release. Such behavior is predicted for all models in which sarcolemmal  $\text{Ca}^{2+}$  influx and SR  $\text{Ca}^{2+}$  release are directed into a single compartment (referred to as “common pool” models).

Our previous model of cardiac calcium handling incorporated an improved description of the L-type  $\text{Ca}^{2+}$  channels and CICR release from ryanodine receptor (RyR) channels exhibiting adaptation. Because these channels, as well as the diadic space between the channels, are each represented as ensemble averages, our previous work is an example of a common pool model (Jafri et al., 1998). While this model reproduces important frequency-dependent aspects of cardiac  $\text{Ca}^{2+}$  cycling and high gain, it also exhibits all-or-none rather than graded  $\text{Ca}^{2+}$  release. We hypothesize that much different behavior will result from a stochastic implementation in which individual functional release

units (FRUs), each consisting of dihydropyridine (DHPR) and RyR channels interacting via a local functional unit subspace. This hypothesis assumes that a variable number of independent FRUs can be recruited via a “local control” mechanism to produce graded  $\text{Ca}^{2+}$  release (Stern, 1992; Cannell et al., 1994; Lopez-Lopez et al., 1995). This assumption is consistent with the spatially and temporally localized SR  $\text{Ca}^{2+}$  release events, known as  $\text{Ca}^{2+}$  sparks, that are thought to be the unitary CICR events in cardiac cells (Lipp and Niggli, 1994; Cheng et al., 1993). We assume that single voltage-activated DHPR channels can open nearby RyRs via localized increases of  $[\text{Ca}^{2+}]$  (Cannell et al., 1995; Lopez-Lopez et al., 1995). This system is of sufficiently low order to be run with stochastic (Monte Carlo) simulations, and allows for systematic parameter variation. The model shows robust graded  $\text{Ca}^{2+}$  release and produces behavior consistent with that reported for  $\text{Ca}^{2+}$  sparks.

## METHODS

Fig. 1 shows the model of the functional release unit. The model consists of one DHPR and eight RyR channels communicating via a functional unit subspace. Experimental studies have suggested that a single DHPR opening activates a single functional release unit (Sham et al., 1998; Cannell et al., 1995). The 8:1 RyR/DHPR stoichiometry used is similar to the experimentally determined value of 7.3 (Bers and Stiffel, 1993). Calcium enters the subspace by two pathways: across the sarcolemma via a single DHPR and from the SR via any of eight RyR channels. These two  $\text{Ca}^{2+}$  fluxes are labeled  $J_{\text{DHPR}}$  and  $J_{\text{RyR}}$ , respectively. The subspace is considered to be a single compartment with no spatial  $\text{Ca}^{2+}$  gradients. Therefore, each RyR channel will sense the same  $\text{Ca}^{2+}$  concentration ( $[\text{Ca}^{2+}]_{\text{ss}}$ ) within the subspace. This simplifying assumption is based on previous three-dimensional models of  $\text{Ca}^{2+}$  diffusion near the channel pore. They suggest that

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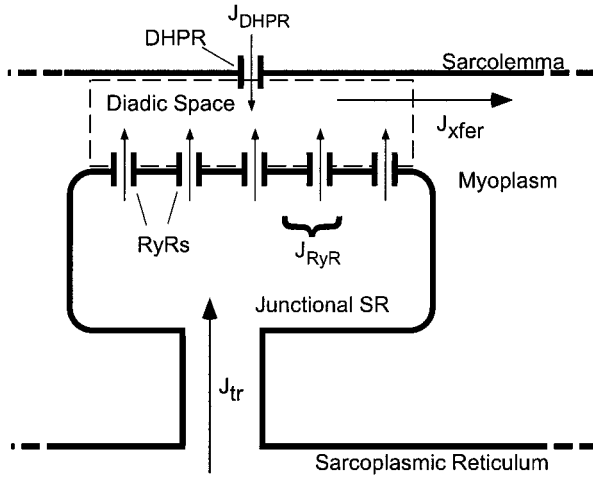


FIGURE 1 Schematic diagram of the functional release unit model.  $\text{Ca}^{2+}$  influx through the DHPR ( $J_{\text{DHPR}}$ ) enters the functional unit subspace (dashed box). This rise in local  $[\text{Ca}^{2+}]$  fosters the opening of one or more of the eight RyR, producing additional influx ( $J_{\text{RyR}}$ ) into the subspace. In this model, the subspace is considered to be a single compartment, hence there is no spatial gradient across this space. Efflux from the subspace ( $J_{\text{xfer}}$ ) occurs via simple diffusion, as does the flux to refill junctional SR ( $J_{\text{tr}}$ ).

$[\text{Ca}^{2+}]$  a short distance away from the channel parallel to the membrane (tens of microseconds) almost instantaneously reaches a uniform spatial profile (Langer and Peskoff, 1996; Soeller and Cannell, 1997; Keizer and Smith, 1998). For simplicity, the myoplasmic  $\text{Ca}^{2+}$  concentration ( $[\text{Ca}^{2+}]_{\text{myo}}$ ) is assumed to be a fixed constant ( $0.1 \mu\text{M}$ ).

We also assume that each FRU behaves independently of others based on experimental findings (Sham et al., 1998; Cannell et al., 1995; Cheng et

al., 1996). Cheng and co-workers observed that  $\text{Ca}^{2+}$  sparks become propagating  $\text{Ca}^{2+}$  waves only under  $\text{Ca}^{2+}$  overload conditions, but not under normal conditions, suggesting that activation does not typically spread from one functional unit to the next. Sparks are also thought to consist of  $\text{Ca}^{2+}$  release from between 6 and 20 RyRs, a finding that is consistent with the RyR/DHPR ratio used in this study. Typically, during a contraction the activation of each functional unit is spread by  $\text{Ca}^{2+}$  entry via the DHPR during depolarization of the sarcolemma.  $\text{Ca}^{2+}$  flux from the subspace to myoplasm ( $J_{\text{xfer}}$ ) is computed as the  $[\text{Ca}^{2+}]$  gradient divided by the relaxation time constant ( $\tau_{\text{xfer}}$ ):

$$J_{\text{xfer}} = \frac{1}{\tau_{\text{xfer}}} ([\text{Ca}^{2+}]_{\text{SS}} - [\text{Ca}^{2+}]_{\text{myo}}) \quad (1)$$

The  $\text{Ca}^{2+}$  flux ( $J_{\text{tr}}$ ) that refills the junctional SR (JSR) is computed as the  $[\text{Ca}^{2+}]$  gradient divided by the relaxation time constant ( $\tau_{\text{tr}}$ ):

$$J_{\text{tr}} = \frac{1}{\tau_{\text{tr}}} ([\text{Ca}^{2+}]_{\text{NSR}} - [\text{Ca}^{2+}]_{\text{JSR}}) \quad (2)$$

where  $[\text{Ca}^{2+}]_{\text{JSR}}$  is the JSR  $\text{Ca}^{2+}$  concentration and  $[\text{Ca}^{2+}]_{\text{NSR}}$  is the network SR (NSR)  $\text{Ca}^{2+}$  concentration. It is assumed that the activation of an individual FRU does not have a significant impact on the total  $[\text{Ca}^{2+}]_{\text{NSR}}$ . Hence,  $[\text{Ca}^{2+}]_{\text{NSR}}$  is a constant ( $[\text{Ca}^{2+}]_{\text{NSR}} = 800 \mu\text{M}$  in the default model).

The DHPR channel is represented by a mode-switching model that was developed previously (Jafri et al., 1998). A state diagram of the mode switching and voltage activation is shown in Fig. 2 A. Transition rates are given in Table 1. The upper and lower rows of states comprise Mode Normal and Mode Ca, respectively. The channel is assumed to be composed of four independent subunits that can each close the channel. This dictates five closed states ( $C_0$ - $C_4$ ) on the top row and a mirror set of closed states ( $C_{\text{Ca}0}$ - $C_{\text{Ca}4}$ ) on the bottom row. The proportionality of the forward and reverse rates between the closed states is dictated by the four-way symmetry assumed for channel subunits. Voltage-dependent activation is incorporated through the rate constants  $\alpha$  and  $\beta$ , which are increasing and

### A. State Diagram of DHPR Channel

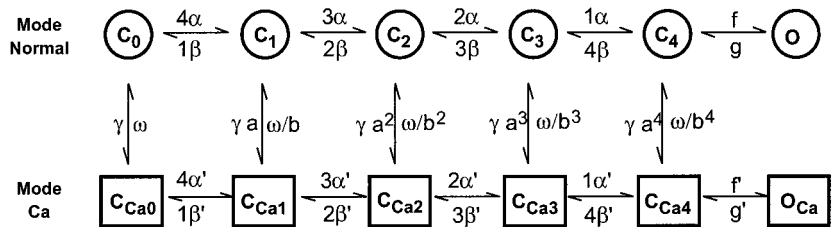
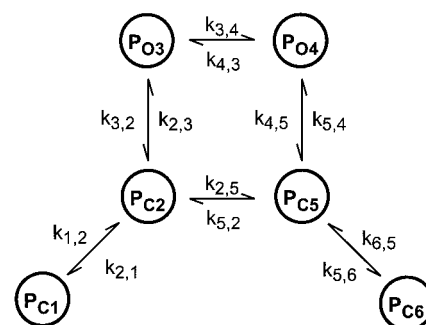


FIGURE 2 State diagrams for the DHPR and RyR channel Markov models. (A) A state diagram of the mode switching and voltage activation of DHPR channel model. The upper row of states comprises Mode Normal and the lower row comprises Mode Ca. The channel is composed for four independent subunits, each of which can close the channel. The corresponding states are  $C_n$ , where  $n$  is the number of permissive subunits. With depolarization, the channels undergo transitions from left to right. With four permissive subunits ( $C_4$ ), there is a voltage-independent transition to the conducting state O. With elevation of  $[\text{Ca}^{2+}]$  the channel transition occurs from the Mode Normal (top) to Mode Ca (bottom).  $f \ll f'$  so that transitions into  $O_{\text{Ca}}$  are rare, which effectively inactivates the channel in Mode Ca. (B) A state model for the RyR with adaptation. The states  $P_{C1}$  and  $P_{C2}$  are the resting states,  $P_{O3}$  and  $P_{O4}$  are the open states, and  $P_{C5}$  and  $P_{C6}$  are the adapted or refractory states. The transitions governed by the rates  $k_{1,2}$ ,  $k_{2,3}$ ,  $k_{3,4}$ ,  $k_{5,4}$ ,  $k_{5,6}$ , and  $k_{2,5}$  are all  $\text{Ca}^{2+}$ -dependent (see Table 2 for values of the rate constants).

### B. State Diagram of RyR Channel



**TABLE 1** DHPR transition probabilities

$\gamma = 0.1875 [\text{Ca}_{\text{SS}}] \text{ s}^{-1}$	$a = 2.0 \text{ s}^{-1}$
$\alpha = 0.4 e^{(V+6)/25} \text{ s}^{-1}$	$b = 2.0 \text{ s}^{-1}$
$\beta = 0.05 e^{-(V+6)/29} \text{ s}^{-1}$	$f = 300.0 \text{ s}^{-1}$
$\alpha' = \alpha a \text{ s}^{-1}$	$g = 2000.0 \text{ s}^{-1}$
$\beta' = (\beta/b) \text{ s}^{-1}$	$f' = 5.0 \text{ s}^{-1}$
$\omega = 10.0 \text{ s}^{-1}$	$g' = 7000.0 \text{ s}^{-1}$
$y_{\infty} = 0.02 + \frac{1}{1 + e^{(V+55)/7.5}} + \frac{0.1}{1 + e^{(V-21)/6}}$	
$\tau_y = 0.02 + \frac{0.04}{1 + e^{(V+30)/9.5}}$	

decreasing functions of voltage, respectively. When in the rightmost closed states ( $C_4$  or  $C_{\text{Ca}4}$ ), there are voltage-independent transitions to the open states ( $O$  or  $O_{\text{Ca}}$ ). Note that  $f'$  is 500 times slower than  $f$ , so that openings are rare in Mode Ca, effectively inactivating the channel.

Transitions to Mode Ca are controlled by  $\gamma$ , which is a function of  $\text{Ca}^{2+}$ . Moving rightward in Fig. 2 A, there are incremental increases in the multiplier of  $\gamma$  and the divisor on  $\omega$ . The effect of this is to greatly increase the transition rate to Mode Ca at high voltages when the channel is opening. The close symmetry between Mode Normal and Mode Ca closed states and similarity of rates (i.e.,  $g$  versus  $g'$ ) is dictated by the experimental finding that gating currents are very similar in the Mode Normal and Mode Ca cases, and by thermodynamic microscopic reversibility. Microscopic reversibility requires that for each cycle the product of rates is equal, whether taken in the clockwise or the counterclockwise direction. Voltage-dependent inactivation is modeled as a Hodgkin-Huxley-type gate ( $y$ ). This gate can inactivate the channel independently of the states discussed above. The equations modeling the DHPR are provided in Table 1.

$\text{Ca}^{2+}$  flux through the DHPR channel ( $J_{\text{DHPR}}$ ) is computed as

$$J_{\text{DHPR}} = \frac{\bar{I}_{\text{DHPR}} \text{DHPR}_{\text{open}}}{2FV_{\text{SS}}} \quad (3)$$

where  $\bar{I}_{\text{DHPR}}$  is open channel current ( $\mu\text{A } \mu\text{F}^{-1}$ ) given by

$$\bar{I}_{\text{DHPR}} = \bar{P}_{\text{Ca}} 4 \frac{VF^2}{RT} \frac{0.001 e^{2VF/RT} - 0.341 [\text{Ca}^{2+}]_0}{e^{2VF/RT} - 1}; \quad (4)$$

$\text{DHPR}_{\text{open}}$  is 1 for states  $O$  or  $O_{\text{Ca}}$ , and is 0 otherwise;  $F$  is Faraday's constant, and  $V_{\text{SS}}$  is the volume of the FRU subspace. The number 0.341 is the activity coefficient of  $\text{Ca}^{2+}$  at the outer opening of the cell. The number 0.001 reflects the product of the activity coefficient of  $\text{Ca}^{2+}$  at the mouth of the channel in the FRU subspace and  $[\text{Ca}^{2+}]_{\text{SS}}$ .

The RyR channel is represented using a model developed by Keizer and Smith (1998). This model was developed to replicate open and dwell times of isolated RyR channels in vitro and in vivo, as well as measured peak and plateau open probabilities with  $\text{Ca}^{2+}$  or cesium ( $\text{Cs}^{2+}$ ) as the charge carrier. The latter measurements describe the adaptive behavior of the RyR channel. As originally described, adaptation is a property of the RyR where, after rapid activation by a step increase in  $[\text{Ca}^{2+}]$ , the channel undergoes a slow spontaneous decrease in open probability (Györke and Fill, 1993). Closing of the RyR has also been attributed to inactivation (Fabiato, 1985b; Sham et al., 1999). In isolated bilayers, adaptation occurs within milliseconds, while inactivation occurs within a few seconds

(Keizer and Levine, 1996). Hence, in this model we are interested in the effects of adaptation on RyR  $\text{Ca}^{2+}$  release.

A state diagram of the RyR model is shown in Fig. 2 B. The state  $P_{03}$  and  $P_{04}$  are open states whereas states  $P_{C1}$ ,  $P_{C2}$ ,  $P_{C5}$ , and  $P_{C6}$  are closed states. Briefly,  $P_{C1}$  and  $P_{C2}$  represent the initial closed states. With an increase in  $[\text{Ca}^{2+}]$ , the channel opens, moving to states  $P_{03}$  and  $P_{04}$ . The other states,  $P_{C5}$ , and  $P_{C6}$ , represent the adapted or refractory state. Transition rates between the states are given by  $k_{x,y}$ , and are provided in Table 3. In the original model (Keizer and Smith, 1998), the charge carrier could be  $\text{Ca}^{2+}$  or  $\text{Cs}^{2+}$ , so that some transition rates depended on  $[\text{Ca}^{2+}]$  in the microdomain around the channel while others depended on the bulk myoplasmic  $[\text{Ca}^{2+}]$ . We assume the charge carrier is  $\text{Ca}^{2+}$  so all rates depend on the  $[\text{Ca}^{2+}]$  in the microdomain. Furthermore, we have modified the rates so that 1) they are scaled to depend on FRU subspace  $\text{Ca}^{2+}$  and not on bulk myoplasmic  $\text{Ca}^{2+}$ , and 2) they are saturating functions of  $\text{Ca}^{2+}$  following Michaelis-Menten kinetics. The new description was derived to match the original description over low levels of  $[\text{Ca}^{2+}]$ , but prevents extremely large, and likely unrealistic, transition rates at high  $[\text{Ca}^{2+}]$ . Such high rates would require extremely small time steps that greatly increase computation time. The results of both these modifications are shown in Table 2.

The  $\text{Ca}^{2+}$  flux through the RyR channels ( $J_{\text{RyR}}$ ) is computed as

$$J_{\text{RyR}} = \sum_{i=1}^8 \bar{J}_{\text{RyR}} \text{RyR}_{\text{open}}^i ([\text{Ca}]_{\text{JSR}} - [\text{Ca}]_{\text{SS}}) \quad (5)$$

where  $\bar{J}_{\text{RyR}}$  is the channel permeability to  $\text{Ca}^{2+}$ ,  $\text{RyR}_{\text{open}}^i$  is 1 when the  $i$ th channel is in state  $P_{03}$  or  $P_{04}$  and 0 otherwise, and  $([\text{Ca}^{2+}]_{\text{SS}} - [\text{Ca}^{2+}]_{\text{JSR}})$  is the driving force from the JSR to the subspace.

The full  $\text{Ca}^{2+}$  balance equations for the subspace and the JSR are

$$\frac{d[\text{Ca}^{2+}]_{\text{SS}}}{dt} = \beta_{\text{SS}} \left( J_{\text{DHPR}} + J_{\text{RyR}} + \frac{V_{\text{myo}}}{V_{\text{SS}}} J_{\text{Xfer}} \right) \quad (6)$$

and

$$\frac{d[\text{Ca}^{2+}]_{\text{JSR}}}{dt} = \beta_{\text{JSR}} \left( J_{\text{tr}} - \frac{V_{\text{SS}}}{V_{\text{JSR}}} J_{\text{RyR}} \right), \quad (7)$$

where

$$\beta_{\text{SS}} = \left( 1 + \frac{[\text{B}]_{\text{SR}} K_{\text{BSR}}}{(K_{\text{BSR}} + [\text{Ca}^{2+}]_{\text{SS}})^2} + \frac{[\text{B}]_{\text{SL}} K_{\text{BSL}}}{(K_{\text{BSL}} + [\text{Ca}^{2+}]_{\text{SS}})^2} \right)^{-1} \quad (8)$$

and

$$\beta_{\text{JSR}} = \left( 1 + \frac{[\text{CSQN}]_{\text{total}} K_{\text{CSQN}}}{(K_{\text{CSQN}} + [\text{Ca}^{2+}]_{\text{JSR}})^2} \right)^{-1} \quad (9)$$

describe the buffering of  $\text{Ca}^{2+}$  using the rapid buffer approximation (Wagner and Keizer, 1994) with  $\beta_{\text{SS}}$  describing buffering in the subspace and  $\beta_{\text{JSR}}$  describing buffering in the JSR. In the subspace there is buffering by the negatively charged phospholipid headgroups in the sarcolemma and the SR membrane. These are approximated as having fixed concentrations, and  $\text{Ca}^{2+}$  dissociation constants are given by  $[\text{B}]_{\text{SL}}$  and  $K_{\text{BSL}}$  for the

**TABLE 2** RyR transition probabilities

$k_{1,2} = 3.0 \times 10^6 [\text{Ca}_{\text{SS}}]^4 / \{(2.68)^4 + [\text{Ca}_{\text{SS}}]^4\} \text{ s}^{-1}$	$k_{5,4} = 198.0 [\text{Ca}_{\text{SS}}]^4 / \{(2.68)^4 + [\text{Ca}_{\text{SS}}]^4\} \text{ s}^{-1}$
$k_{2,1} = 2.5 \times 10^5 \text{ s}^{-1}$	$k_{4,5} = 66.67 \text{ s}^{-1}$
$k_{2,3} = 3.0 \times 10^7 [\text{Ca}_{\text{SS}}]^4 / \{(2.68)^4 + [\text{Ca}_{\text{SS}}]^4\} \text{ s}^{-1}$	$k_{2,5} = 3.0 \times 10^5 [\text{Ca}_{\text{SS}}]^4 / \{(2.68)^4 + [\text{Ca}_{\text{SS}}]^4\} \text{ s}^{-1}$
$k_{3,2} = 9.6 \times 10^3 \text{ s}^{-1}$	$k_{5,2} = 1.235 \text{ s}^{-1}$
$k_{3,4} = 3.0 \times 10^6 [\text{Ca}_{\text{SS}}]^4 / \{(2.68)^4 + [\text{Ca}_{\text{SS}}]^4\} \text{ s}^{-1}$	$k_{5,6} = 3.0 \times 10^6 [\text{Ca}_{\text{SS}}]^4 / \{(2.68)^4 + [\text{Ca}_{\text{SS}}]^4\} \text{ s}^{-1}$
$k_{4,3} = 1.3 \times 10^4 \text{ s}^{-1}$	$k_{6,5} = 3.0 \times 10^6 \text{ s}^{-1}$

TABLE 3 Parameters

$V_{SS} = 2.03 \times 10^{-12} \mu\text{L}$	$[B_{SL}] = 1124.0 \mu\text{M}$
$V_{JSR} = 1.05 \times 10^{-10} \mu\text{L}$	$K_{BSL} = 8.7 \mu\text{M}$
$[\text{Ca}^{2+}]_{\text{myo}} = 0.1 \mu\text{M}$	$[\text{CSQN}]_{\text{total}} = 15.0 \text{ mM}$
$[\text{Ca}^{2+}]_{\text{NSR}} = 800 \mu\text{M}$	$K_{\text{CSQN}} = 0.8 \text{ mM}$
$[\text{Ca}^{2+}]_o = 1.8 \text{ mM}$	$F = 96500 \text{ coul (mol } e^-)^{-1}$
$\tau_{\text{tr}} = 0.005 \text{ ms}$	$T = 310 \text{ K}$
$\tau_{\text{xfer}} = 0.0007 \text{ ms}$	$R = 8.314 \text{ J mol}^{-1} \text{ K}^{-1}$
$[B_{SR}] = 47.0 \mu\text{M}$	$\bar{J}_{\text{RyR}} = 3960.0 \text{ s}^{-1}$
$K_{\text{BSR}} = 0.87 \mu\text{M}$	$\bar{P}_{\text{Ca}} = 1.51 \times 10^{-11} \text{ cm ms}^{-1}$

sarcolemma and  $[B]_{\text{SR}}$  and  $K_{\text{BSR}}$  for the SR (Smith et al., 1998). In the JSR, calsequestrin (CSQN) is assumed to be the only significant  $\text{Ca}^{2+}$  buffer (Luo and Rudy, 1994).

Monte Carlo simulations are run using standard methods for Markov processes (Keizer, 1987). Unless noted otherwise, all simulations use a voltage clamp protocol. Specifically, the model is allowed a period of time (0.1 s) to reach steady state at a holding potential of  $-80 \text{ mV}$ , followed by a voltage step to a test potential for 0.2 s, and then returned to the  $-80 \text{ mV}$  holding potential. Each trial is repeated 500 times before changing the voltage step (typically increased from  $-50$  and  $+50 \text{ mV}$  in  $5\text{-mV}$  increments). Results are averaged over the 500 independent trials at each voltage, hence could be considered the ensemble behavior of 500 independent functional units. This number is probably less than the total number of functional units in a cell, which is estimated to be in the range of  $10^3$ – $10^4$  (Isenberg, 1995). This number was selected to yield a reasonable compromise between minimization of run time and reduction of variability in the results.

## RESULTS

Sample Monte Carlo results are shown in Fig. 3 for a single trial with a voltage step to  $0 \text{ mV}$ . The peak fluxes are shown for the DHPR channel (*solid line*) and the sum of the eight RyRs (*dashed line*) in Fig. 3 *A*. After a voltage transition to  $0 \text{ mV}$  at time  $0.1 \text{ s}$ , the DHPR might open (Fig. 3 *A*). In the simulation shown, the DHPR opens only once. Often there will be no openings and sometimes more than one opening. The DHPR flux displays a consistent level of peak flux for a given clamp voltage, because we assume a single channel with constant flux that depends only the clamp voltage. In contrast, the RyR show a variable level of flux because 1) a subset of eight channels is open at any given time; and 2) the driving force for  $\text{Ca}^{2+}$  flux depends on  $[\text{Ca}^{2+}]_{\text{JSR}}$ , which varies with time. Note that RyR flux is largest at the beginning of the voltage step, reflecting a relatively large driving force and higher open probability early in the  $\text{Ca}^{2+}$  release event. This effect can also be seen in Fig. 3 *B*, where the flux is integrated over time to produce the total integrated flux of  $\text{Ca}^{2+}$  into the subspace from each of the two possible sources. Fig. 3, *C* and *D* show the corresponding changes in  $\text{Ca}^{2+}$  concentration in the subspace ( $[\text{Ca}^{2+}]_{\text{SS}}$ ) and the JSR ( $[\text{Ca}^{2+}]_{\text{JSR}}$ ), respectively. The peak  $[\text{Ca}^{2+}]_{\text{SS}}$  reaches a value of  $\sim 22 \mu\text{M}$ . The local JSR depletes from  $800$  to  $\sim 400 \mu\text{M}$ .

While Fig. 3 shows results for a single trial, Fig. 4 shows similar data averaged over 500 independent runs. The average peak and integrated flux through DHPR (*lower line*) and RyRs (*upper line*) are shown in Fig. 4, *A* and *B*,

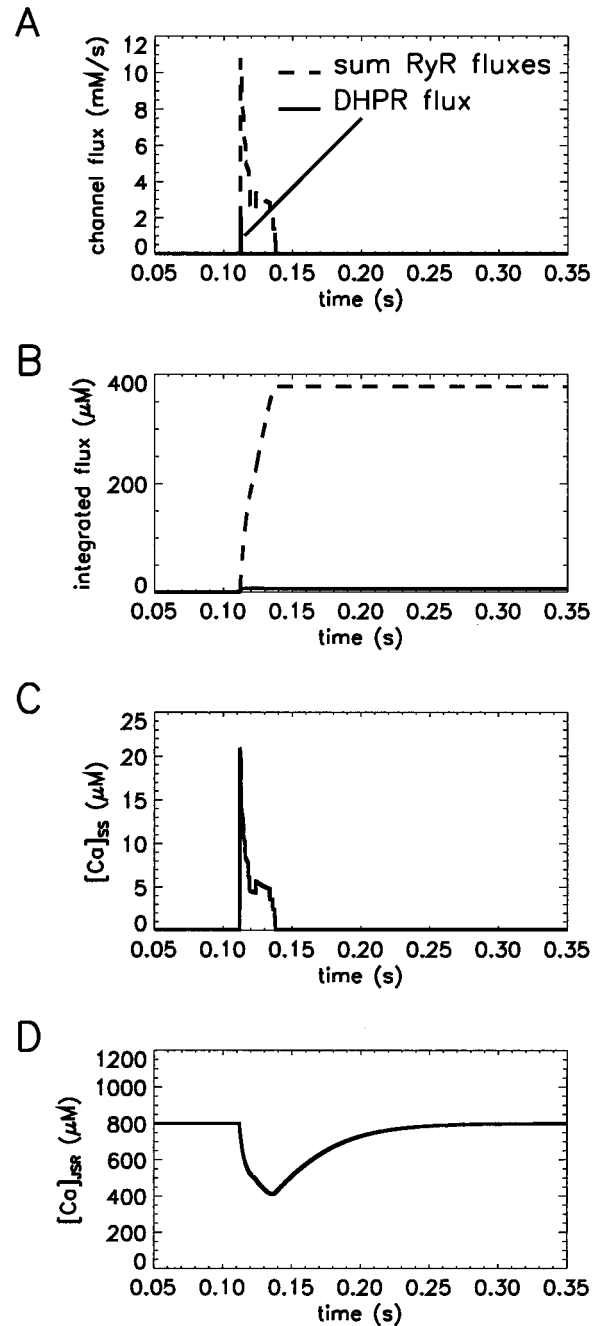


FIGURE 3 Sample results for a single functional unit driven by a voltage step to  $0 \text{ mV}$  from  $0.1$  to  $0.3 \text{ s}$ . (*A*) Peak fluxes are shown for the DHPR channel (*solid line*) and the sum of the eight RyRs (*dashed line*). (*B*) Integrated fluxes are shown for the DHPR channel (*solid line*) and the sum of the eight RyRs (*dashed line*). (*C*) The changes in  $\text{Ca}^{2+}$  concentration in the subspace ( $[\text{Ca}^{2+}]_{\text{SS}}$ ). (*D*) The changes in JSR  $\text{Ca}^{2+}$  concentration ( $[\text{Ca}^{2+}]_{\text{JSR}}$ ) indicates the degree to which SR empties during a  $\text{Ca}^{2+}$  release event.

respectively. In both cases, the magnitude of the averaged data is somewhat lower than the corresponding single channel data because of the occurrence of runs in which the DHPR channel does not open, thus producing no RyR openings. Fig. 4, *C* and *D* show the corresponding average



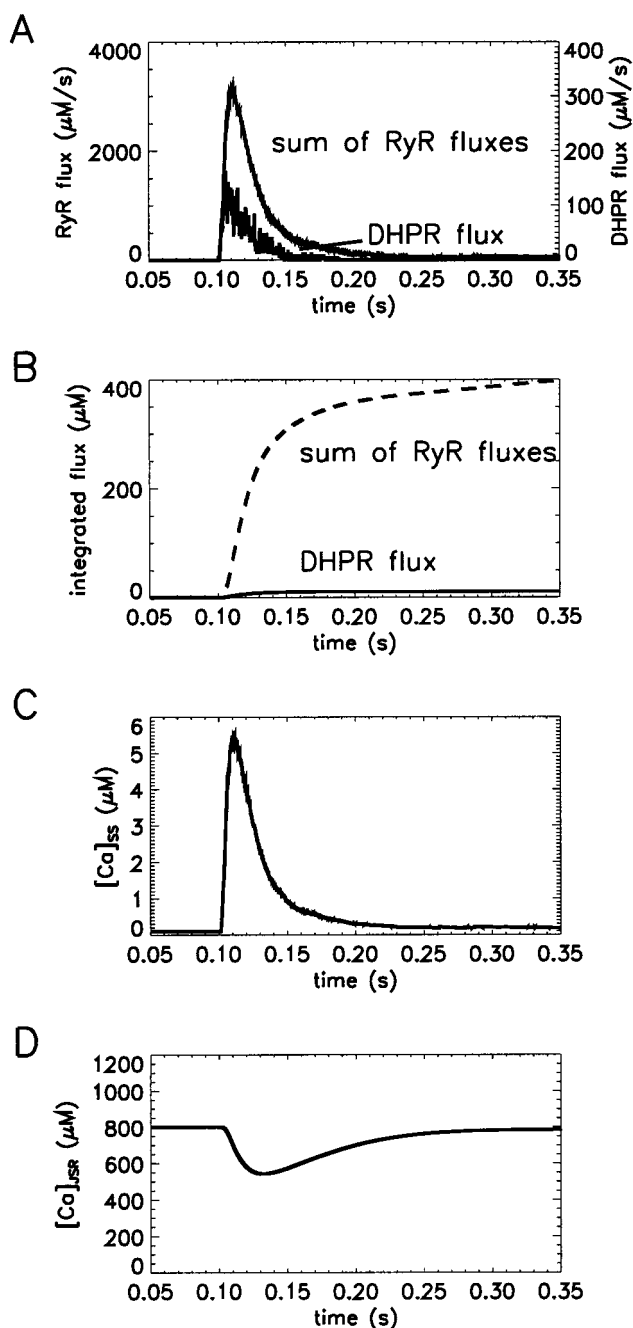


FIGURE 4 Average results for 500 single runs (same protocol as used in Fig. 3 for a single functional unit driven by a voltage step to 0 mV from 0.1 to 0.3 s. (A) Average peak fluxes are shown for the DHPR channel and the sum of the eight RyRs. (B) Average integrated fluxes are shown for the DHPR channel (solid line) and the sum of the eight RyRs (dashed line). (C) The changes in average  $\text{Ca}^{2+}$  concentration in the subpace ( $[\text{Ca}^{2+}]_{ss}$ ). (D) The changes in average JSR  $\text{Ca}^{2+}$  concentration ( $[\text{Ca}^{2+}]_{JSR}$ ) indicate the degree to which SR empties during a  $\text{Ca}^{2+}$  release event.

changes in  $[\text{Ca}^{2+}]_{ss}$  and  $[\text{Ca}^{2+}]_{JSR}$ . The change in  $[\text{Ca}^{2+}]_{JSR}$  from a resting value of 800 to 562  $\mu\text{M}$  was a decrease of 38%. A similar decrease is observed experimentally as cardiac myocytes retain 35% of their resting SR  $\text{Ca}^{2+}$  during a contraction under normal SR loading conditions (Bassani et al., 1995a).

Again, the data are smoother and show smaller changes in magnitude when compared to the corresponding data for a single functional unit in Fig. 3. These results demonstrate that the model produces positive gain, i.e., average integrated flux through the RyRs is  $\sim 10$  times larger than that through the DHPR.

The next question to address is whether  $\text{Ca}^{2+}$  release is graded with influx of trigger  $\text{Ca}^{2+}$  through the DHPR. To test gradedness, the step potential is varied from  $-50$  to  $+50$  mV in 5-mV increments. When plotted against clamp voltage, the averaged DHPR fluxes produce bell-shaped profiles for both integrated (Fig. 5 A, solid line) and peak fluxes (Fig. 5 C, solid line). The peak of the DHPR flux is  $\sim -10$  mV, similar to that measured experimentally. Likewise, RyR flux (dashed lines) shows similar bell-shaped profiles, but are much larger in amplitude. These data clearly show that the model can reproduce both high gain and graded  $\text{Ca}^{2+}$  release that is observed in cardiac myocytes. The gain or amplification factor is defined as the ratio of the RyR flux to the DHPR flux. It shows the amount of amplification of the trigger  $\text{Ca}^{2+}$  by CICR. The gain for the integrated fluxes is shown in Fig. 5 B and the gain for the peak flux is shown in Fig. 5 D. While the gain shown is in the range observed physiologically (Wier et al., 1994), the shape differs from that seen in the experiments. Possible explanations for this will be described in the Discussion.

In DHPR channels, separate features produce the rising and falling phases of the bell-shaped flux profile. The rising phase is produced by the increasing open probability and results from voltage-sensitive channel activation. The declining phase reflects changes in open-channel current. The two phases of the RyR flux curves also reflect this dual modulation. This is demonstrated in the next set of simulations. In Fig. 6 A, the activation function of the DHPR channel is shifted by  $-10$  and  $+10$  mV, producing shifts of the rising edge of the peak DHPR flux functions (seen by the three low-amplitude curves in Fig. 6 A). The rising phases of the RyR peak flux functions show corresponding shifts (seen by the three higher amplitude curves in Fig. 6 A). Note that there are only small changes in the declining phases because the open probability of the DHPR is close to its saturating level. The declining phase predominantly reflects the open-channel I-V relation of the DHPR functions. As shown in Fig. 6 B, shifting the open-channel I-V relation by  $-10$  and  $+10$  mV produces corresponding changes in both DHPR and RyR flux functions. These results indicate that properties of the RyR release flux are closely coupled to processes governing activation and permeation of the DHPR.

The next set of simulations addresses the role of adaptation of RyR  $\text{Ca}^{2+}$  release. RyR adaptation rate is first increased and then decreased by a factor of 5 by adjusting the transition rates  $k_{4,5}$  and  $k_{2,5}$  (see Fig. 2 B). A slower adaptation rate increases peak RyR flux and  $[\text{Ca}^{2+}]$  in the subpace (Fig. 7, A and B, dotted lines). Conversely, the effect of more rapid adaptation is to decrease both peak flux and  $[\text{Ca}^{2+}]_{ss}$  (Fig. 7, A and B, dashed lines). It is also clear

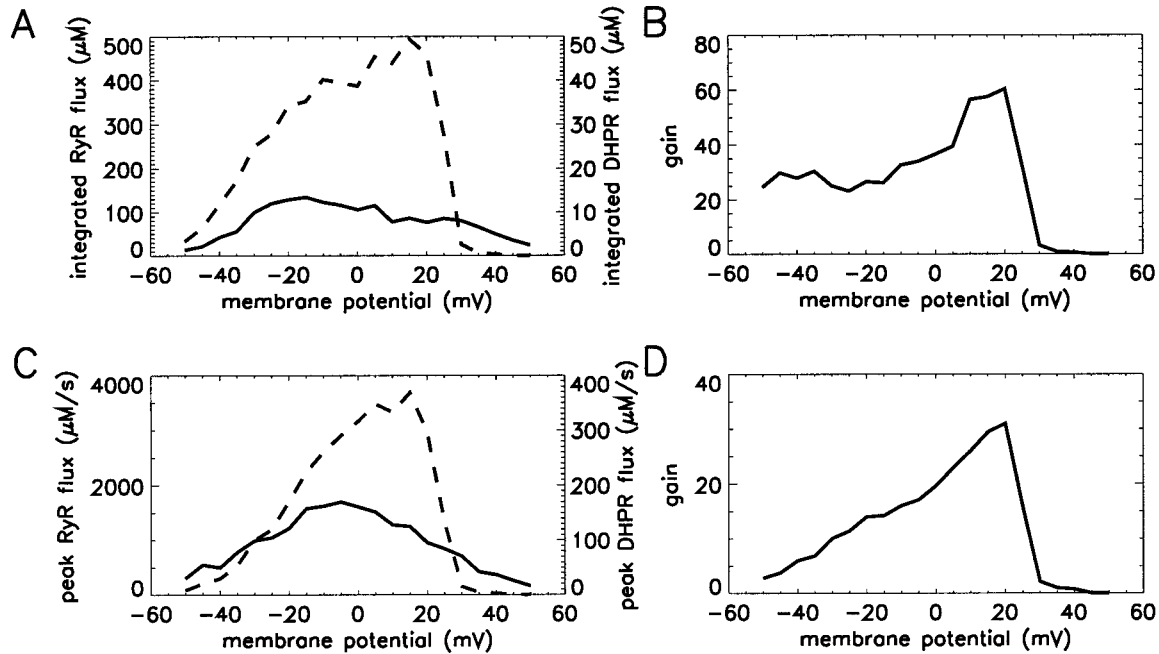


FIGURE 5 Model exhibits positive gain and graded  $\text{Ca}^{2+}$  release. To modulate the amount of trigger  $\text{Ca}^{2+}$ , voltage pulses are changed in 5-mV steps from -50 to 50 mV. The data are averaged from 500 runs. (A) Integrated flux through the DHPR (solid line) shows a bell-shaped profile, similar to those measured experimentally. The integrated RyR  $\text{Ca}^{2+}$  release (dashed line) also has a bell-shaped profile, which shows gradedness and is much larger, that demonstrates positive gain. (B) The gain or amplification factor for the integrated fluxes. (C) Peak flux shows very similar behavior, although there are slight differences in the shapes of the curves when compared to the integrated flux data. (D) The gain for the peak fluxes.

that rapid adaptation produces a model with a significantly decreased gain that is smaller than that observed experimentally (Wier et al., 1994). This finding suggests that measurements of gain may help to limit estimates of RyR adaptation rates.

The effect of RyR adaptation on JSR  $\text{Ca}^{2+}$  concentration is examined in Fig. 7 C. Slowed adaptation produces a larger SR  $\text{Ca}^{2+}$  release and lower  $[\text{Ca}^{2+}]_{\text{JSR}}$  during the course of the  $\text{Ca}^{2+}$  release (dotted line). A more rapid adaptation rate produces a smaller SR  $\text{Ca}^{2+}$  release and higher  $[\text{Ca}^{2+}]_{\text{JSR}}$  during the course of the  $\text{Ca}^{2+}$  release (dashed line). Therefore, in this model, RyR adaptation rate has an effect on the level of SR emptying and contributes to termination of SR  $\text{Ca}^{2+}$  release.

Considerable experimental evidence suggests that SR  $\text{Ca}^{2+}$  release is positively correlated with the  $\text{Ca}^{2+}$  load (Bers, 1991; Bassani et al., 1995a; Janczewski et al., 1995). For example, by decreasing the SR  $\text{Ca}^{2+}$  content by 56%, its control value reduces the RyR  $\text{Ca}^{2+}$  release by 52% (Janczewski et al., 1995). The effect of altered SR  $\text{Ca}^{2+}$  load is tested in the model by changing the initial  $\text{Ca}^{2+}$  concentration of JSR ( $[\text{Ca}^{2+}]_{\text{JSR}}$ ) and the concentration of the store that refills SR ( $[\text{Ca}^{2+}]_{\text{NSR}}$ ). When SR  $\text{Ca}^{2+}$  load is doubled from the control value (1600  $\mu\text{M}$  vs. 800  $\mu\text{M}$ ), the peak flux increases over the entire range of voltages tested (Fig. 8 A, dashed line). Similarly, when SR  $\text{Ca}^{2+}$  load is halved from the control value (400  $\mu\text{M}$  vs. 800  $\mu\text{M}$ ), the peak flux decreases (Fig. 8 A, dashed line).

The change in SR load also produces large changes in the temporal behavior of SR  $\text{Ca}^{2+}$  release. As shown in Fig. 8

B, reduced SR load (dotted line) produces a smaller, shorter peak in  $[\text{Ca}^{2+}]_{\text{SS}}$  with a smaller sustained component after the  $\text{Ca}^{2+}$  release. In contrast, increased SR load produces a larger magnitude of  $\text{Ca}^{2+}$  release with an elevated sustained component.  $\text{Ca}^{2+}$  release also continues after the voltage step (see dashed line after the voltage step from 0.1–0.3 s in Fig. 8 B). This phenomenon occurs only when SR  $\text{Ca}^{2+}$  load is elevated so that release become regenerative as RyRs continue to activate each other (i.e., the cluster bomb effect as described by Stern (1992)).

In contrast to regenerative RyR openings, the data of Fig. 8 demonstrate that model RyR  $\text{Ca}^{2+}$  release closely follows the DHPR openings. It has been pointed out elsewhere (Callewaert, 1992; Stern, 1992) that such a system produces high gain and graded  $\text{Ca}^{2+}$  release. However, the data of Fig. 8 B also show that under at least some conditions (i.e., high SR load), RyR  $\text{Ca}^{2+}$  release can be sustained in the absence of influx of trigger  $\text{Ca}^{2+}$ .

In the next set of simulations, we seek to determine the functional coupling between the DHPR and RyRs as compared to coupling between adjacent RyRs. If the former is much stronger, then RyRs may simply follow the trigger influx. If the latter is strong, then the system is more likely to tend toward self-regenerating RyR  $\text{Ca}^{2+}$  release. To address this issue, the stochastic model is modified so that either a single DHPR or single RyR channel is held open to drive the functional unit in the absence of any other trigger influx of  $\text{Ca}^{2+}$ . An important variable in such simulations is the open duration. Therefore, an initial step is to determine

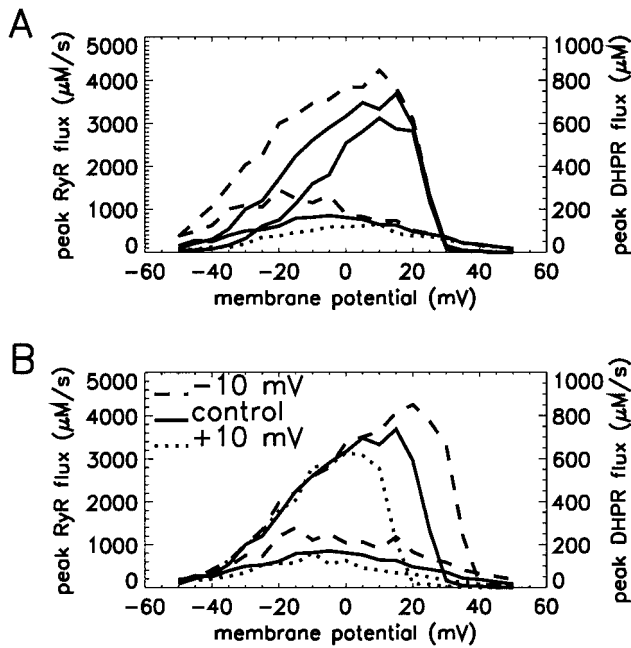


FIGURE 6 The rising phase of the bell-shaped profiles reflects voltage-dependent activation of the DHPR channel, whereas the falling phase reflects the open channel I-V relations. To modulate the amount of trigger  $\text{Ca}^{2+}$ , voltage pulses are changed in 5-mV steps from -50 to 50 mV. The data are averaged from 500 runs. (A) The activation function of the DHPR channel is shifted by -10 (dashed line) and +10 mV (dotted line). The rising phase of the RyR average peak flux curves shows corresponding shifts, showing that RyR  $\text{Ca}^{2+}$  release closely corresponds to DHPR open probability on the rising phase. (B) The I-V relations of the DHPR are shifted by -10 (dashed line) and +10 mV (dotted line). The falling phase of the RyR average peak flux curves show corresponding shifts, showing that RyR  $\text{Ca}^{2+}$  release closely corresponds to DHPR I-V relations on the falling phase.

an appropriate range of channel open times for use in the model.

Fig. 9 shows the channel open times plotted as a function of initial time of the opening event. The model was run using the same standard conditions as in Figs. 3–5. In Fig. 9 A, the DHPR opens times are plotted during the 0.1–0.3-ms voltage step to 0 mV. Most points are below 3 ms, and the distribution of points shows that although there are more frequent openings early in the voltage step, there is no apparent dependence of open time on the time of opening. To see that this is the case, the data points within 1-ms time intervals were averaged, and the result is plotted as a gray line in Fig. 9 A. The line has slope near zero, demonstrating that the DHPR mean open time is constant at  $\sim 0.5$  ms. This corresponds well with the value of 0.45 ms measured experimentally by Rose and co-workers (1992). In Fig. 9 B, the RyR open times show some time dependence with a peak mean open time of  $\sim 6.7$  ms early during the voltage pulse and mean open time of  $\sim 2.8$  ms later in the pulse. These values are in agreement with the ranges of values from 1.5 to 7.1 ms measured experimentally for control conditions (Lukyanenko et al., 1996; Eager and Dulhunty,

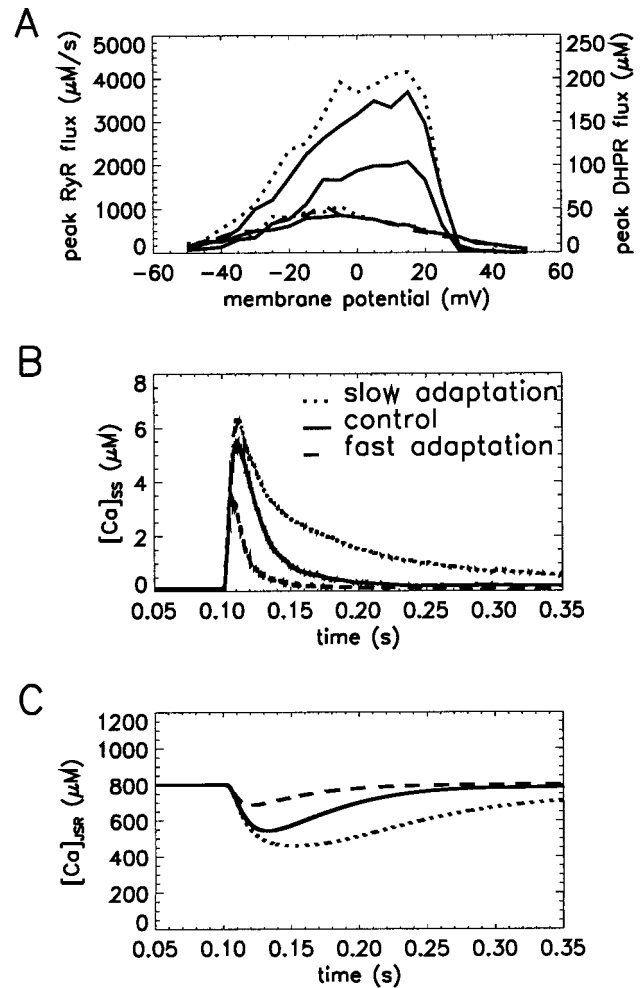


FIGURE 7 The effects of modifying adaptation rate on RyR  $\text{Ca}^{2+}$  release. The transition rates into the adapted state ( $k_{2,5}$  and  $k_{4,5}$  in Fig. 2 B) are increased or decreased by a factor of 10 to increase or decrease adaptation rate, respectively. Data are gathered from voltage pulses from -50 to 50 mV in 5-mV increments, and are averaged from 500 runs at each voltage. (A) Slow adaptation rate (dotted line) produces a larger peak flux than control conditions (solid line), the same as Fig. 5 C). Increased adaptation rate decreases the peak flux. (B) The average  $[\text{Ca}^{2+}]_{ss}$  transients at 0 mV show that adaptation rate effects both the magnitude and temporal profile of RyR  $\text{Ca}^{2+}$  release. (C) The average  $[\text{Ca}^{2+}]_{SR}$  lines show that the higher rate of adaptation (dashed line) decreases the degree of SR unloading during  $\text{Ca}^{2+}$  release, whereas decreased rate (dotted line) produces greater SR unloading.

1998). For 500 runs, the 14,520 RyR openings (Fig. 9 B) are much more numerous than 1567 DHPR openings (Fig. 9 A).

Fig. 10 shows model results when a single DHPR or RyR channel is held open. The average  $\text{Ca}^{2+}$  transients for 500 runs are shown in Fig. 10 A for a DHPR open time of 0.5 ms (black line) and 16.0 ms (gray line). The amplitudes are similar with a slight variation of the time course. This compares well with the experimental results of Sham and co-workers (1998) in which the mean open time of the DHPR is increased from 0.27 ms to 15.9 ms by the addition of the agonist FPL64176. The ensuing  $\text{Ca}^{2+}$  transients caused by  $\text{Ca}^{2+}$  release from the SR are similar in ampli-

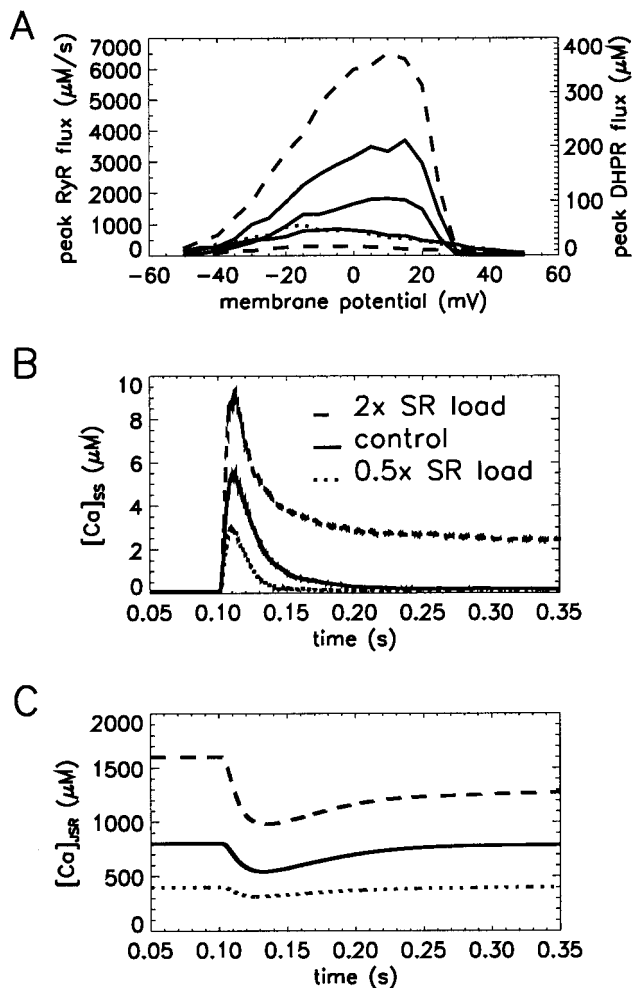


FIGURE 8 The effects of modifying SR  $\text{Ca}^{2+}$  load on RyR  $\text{Ca}^{2+}$  release. The  $[\text{Ca}^{2+}]$  of JSR and the  $[\text{Ca}^{2+}]$  of the refilling store are doubled ( $1600 \mu\text{M}$ ) (dashed line) or halved ( $400 \mu\text{M}$ ) (dotted line) to effectively increase or decrease the SR load. Data are from voltage pulses from  $-50$  to  $50$  mV in  $5$ -mV increments and are averaged from 500 runs at each voltage. (A) Increased SR load (dashed line) produces a larger peak flux than control conditions (solid line), the same as Fig. 5 C). (B) The average  $[\text{Ca}^{2+}]_{\text{ss}}$  transients at  $0$  mV show that SR load effects both the magnitude and temporal profile of RyR  $\text{Ca}^{2+}$  release. Doubling the SR load (dashed line) produces elevated sustained  $\text{Ca}^{2+}$  release during the voltage pulse ( $0.1$ – $0.3$  s) and regenerative RyR  $\text{Ca}^{2+}$  release after the pulse when DHPR influx has ceased. (C) The average  $[\text{Ca}^{2+}]_{\text{Jsr}}$  lines show the degree of SR unloading during and after the voltage pulse.

tude, with the  $\text{Ca}^{2+}$  transient with the agonist being slightly longer in duration. When a single RyR is held open for  $0.5$  ms (black line) and  $16.0$  ms (gray line), there is virtually no difference between the FRU subspace  $\text{Ca}^{2+}$  transients. These simulations are run with the default initial SR  $\text{Ca}^{2+}$  load ( $[\text{Ca}^{2+}]_{\text{Jsr}} = [\text{Ca}^{2+}]_{\text{NSR}} = 800 \mu\text{M}$ ) so the SR load is similar to those during initial portions of the voltage step in previous simulations (Figs. 3–5). The degree of SR unloading is also similar to previous simulations. For the  $5$ - and  $16$ -ms single channel openings, the  $[\text{Ca}^{2+}]_{\text{Jsr}}$  falls to  $370$  and  $394 \mu\text{M}$ , respectively, for the DHPR case and  $376$  and  $394 \mu\text{M}$  for RyR case (data not shown).  $[\text{Ca}^{2+}]_{\text{Jsr}}$  can be

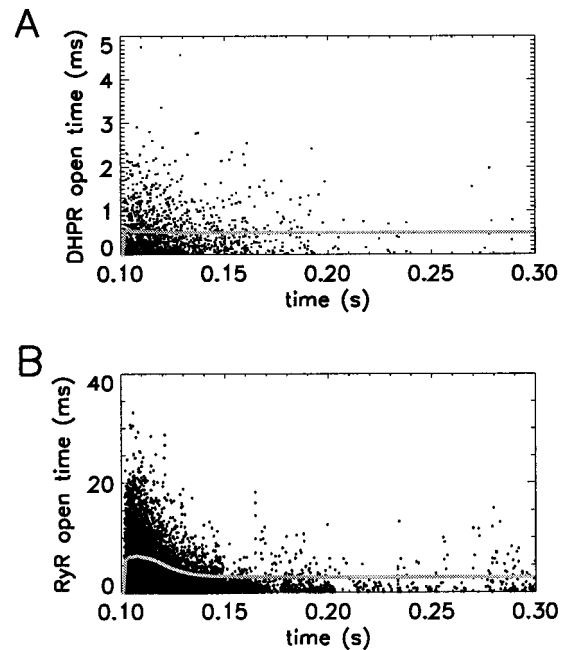


FIGURE 9 The DHPR and RyR open times during a voltage pulse to  $0$  mV under default conditions. The channel open times (ordinate) plotted as a function of initial time of the opening event (abscissa). (A) DHPR open times show little dependence on initial time of opening, as shown by the average for  $1$ -ms bins (white-black line). The mean open time is  $0.50 \pm 0.51$  ms for 1567 points collected from 500 runs. (B) RyR open times show some time-dependence with a peak average open time of  $\sim 6.7$  ms early during the voltage pulse, and average around  $2.8$  ms (white line) later in the clamp. The mean open time is  $2.8 \pm 3.8$  ms for 14,520 points collected from 500 runs.

clamped at  $800 \mu\text{M}$  so that no SR emptying occurs. The corresponding  $\text{Ca}^{2+}$  transients are of similar magnitude, but are over  $10$  times longer ( $>0.6$  s, data not shown). This finding suggests that SR unloading plays an important role in the termination of SR  $\text{Ca}^{2+}$  release.

The above data show that both single DHPR and single RyR openings can trigger  $\text{Ca}^{2+}$  release from adjacent RyRs. This suggests that termination of SR  $\text{Ca}^{2+}$  release may be quite difficult. However, as seen previously in Fig. 4 A, RyR  $\text{Ca}^{2+}$  release stops shortly after DHPR influx ceases. A possible explanation is that RyR open times tend to become shorter during later phases of the voltage pulse (Fig. 9 B), which could produce less activation of neighboring RyRs. However, the possibility that RyR open time alone can lead to less regenerative release is unlikely, given that a  $0.5$ -ms RyR opening still produces a  $\text{Ca}^{2+}$  transient similar to a  $16.0$ -ms RyR opening (Fig. 10 B). A short RyR opening can still be very effective in triggering release from its neighbors in the model.

A more important feature for termination of SR  $\text{Ca}^{2+}$  release is the depletion of SR  $\text{Ca}^{2+}$  that occurs during the voltage step. This is demonstrated by repeating the single channel opening experiments for a range of open times and for a range of SR loads. Results are shown in Fig. 10, C and D. The peak RyR  $\text{Ca}^{2+}$  flux for different values of initial



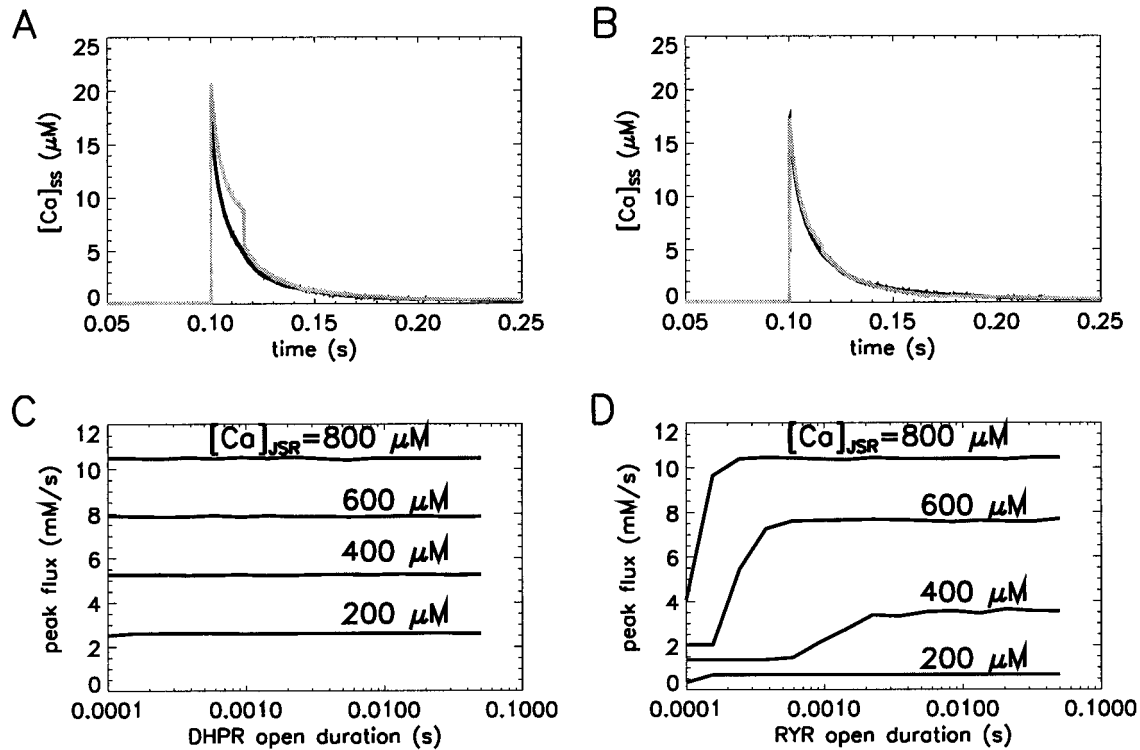


FIGURE 10 The RyR  $\text{Ca}^{2+}$  release elicited from a single DHPR or RyR opening. (A) The average  $\text{Ca}^{2+}$  transients for 200 runs with default initial SR  $\text{Ca}^{2+}$  load ( $[\text{Ca}^{2+}]_{\text{JSR}} = 800 \mu\text{M}$ ). The response for a 0.5 ms (black line) and a 16 ms (gray line) DHPR opening are similar, although the latter is slightly larger and has a small shoulder as a result of the DHPR  $\text{Ca}^{2+}$  influx. (B) The  $\text{Ca}^{2+}$  transients for a single 0.5 ms (black line) or 16 ms (gray line) RyR opening are similar, although slightly smaller than those produced by a single DHPR opening. (C) RyR  $\text{Ca}^{2+}$  release is independent of the open duration of a single DHPR, but highly dependent on SR load. The  $[\text{Ca}^{2+}]$  of JSR and the  $[\text{Ca}^{2+}]$  of the refilling store are set to 800, 600, 400, and 200  $\mu\text{M}$  (as labeled) to vary the SR load. (D) RyR  $\text{Ca}^{2+}$  release shows some dependence on the open duration of a single RyR for short open times. As in (C) above, RyR  $\text{Ca}^{2+}$  release is very dependent on SR load.

$[\text{Ca}]_{\text{JSR}}$  are shown. In Fig. 10 C, the DHPR was held open for a range of open times from 0.1 ms to 50.0 ms. The peak RyR  $\text{Ca}^{2+}$  flux is invariant of DHPR open time, as observed by Sham and co-workers (1998), but depends on the initial SR  $\text{Ca}^{2+}$  concentration. The results show that integrated RyR  $\text{Ca}^{2+}$  flux depends mainly on the  $[\text{Ca}]_{\text{JSR}}$ , with little dependence on open duration. In contrast, DHPR open duration has almost no effect on integrated RyR flux, except at very short open durations. The reason is that as the duration of the DHPR opening increases, the RyR tend to adapt so that further RyR  $\text{Ca}^{2+}$  release is not produced. When the adaptation rate is increased by a factor of 10, integrated RyR flux decreases to  $\sim 10\%$  of the control value, but again with little dependence on DHPR open duration (data not shown). Decreasing adaptation rate by a factor of 10 increases integrated RyR flux by 50%. Again, integrated  $\text{Ca}^{2+}$  release flux shows little dependence on DHPR open duration (data not shown).

In contrast to the DHPR data, RyR open time can strongly influence peak RyR flux. As shown in Fig. 10 D, integrated RyR flux strongly depends on the  $[\text{Ca}]_{\text{JSR}}$ . The higher  $[\text{Ca}]_{\text{JSR}}$ , the greater the peak flux. Integrated RyR flux also increases monotonically with RyR open duration.

The final set of simulations studies the effects of altered FRU subspace geometry on graded  $\text{Ca}^{2+}$  release. These

simulations are motivated by experiments by Gomez and co-workers showing SR  $\text{Ca}^{2+}$  release decreases during congestive heart failure (CHF; Gomez et al., 1997). The researchers observed that the ability of the DHPR to activate SR  $\text{Ca}^{2+}$  release was reduced in the hearts of CHF rats. The suggested that a possible mechanism for this is that the DHPRs and RyRs become functionally uncoupled, possibly as a result of altered geometry in diadic space. Here, we seek to uncouple DHPR and RyRs in the model by one of two ways, increasing FRU subspace volume or increasing the efflux of  $\text{Ca}^{2+}$  out of the FRU subspace.

Fig. 11 shows the effects of altered functional unit subspace volume. Doubling the FRU subspace volume (Fig. 11 A, dashed line) produces a larger peak flux than control conditions (solid line, same as Fig. 5 C), with the peak shifted to lower step potentials. Hence, the larger subspace volume can produce larger release flux at low voltages, but decreases the effectiveness of the DHPR trigger at high voltages. Decreasing the FRU subspace volume by half increases the peak flux and shifts it to higher step potentials (Fig. 11 A, dotted line) compared to the control (solid line). In this case, the small DHPR trigger  $\text{Ca}^{2+}$  influx seen at high voltages is more effective at triggering RyR  $\text{Ca}^{2+}$  release than in the control. However, a smaller subspace produces higher subspace  $[\text{Ca}^{2+}]$  reducing release at lower

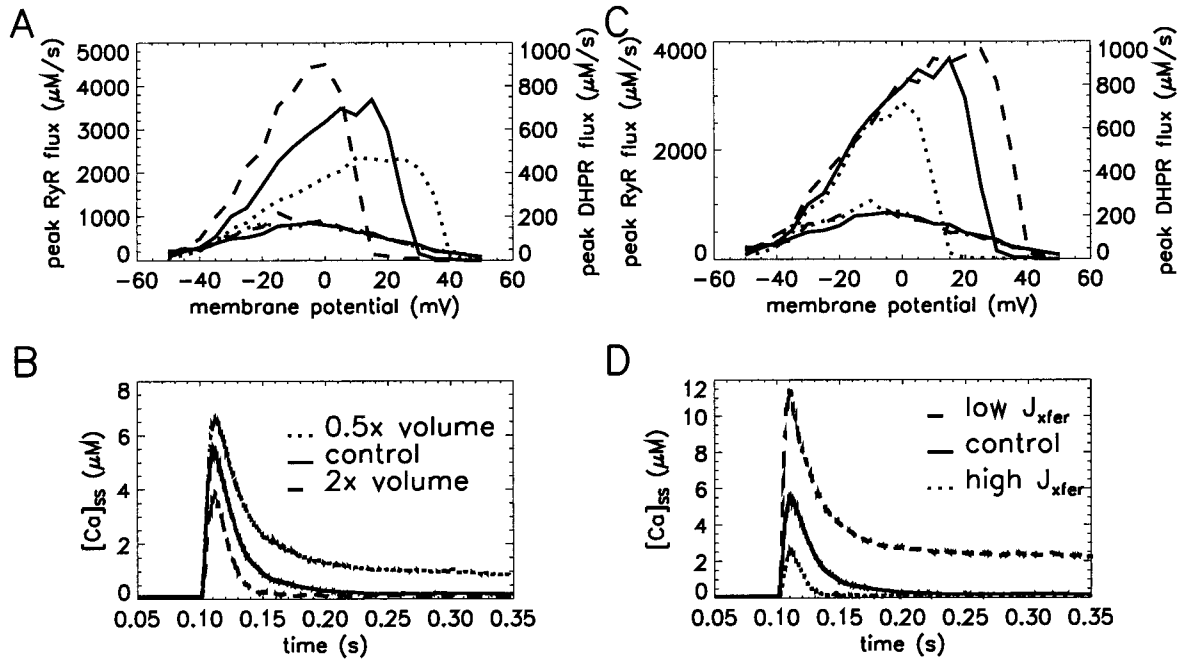


FIGURE 11 The effects of modifying subspace volume on RyR  $\text{Ca}^{2+}$  release. The volume of the subspace is doubled (dashed line) or halved (dotted line). Data are from voltage pulses from  $-50$  to  $50$  mV in  $5$ -mV increments and is averaged from 500 runs at each voltage. (A) Larger subspace (dashed line) produces a larger peak flux than control conditions (solid line), the same as Fig. 5 C), but only at lower voltages. At higher voltages, the trigger influx through the DHPR channel is insufficient to trigger  $\text{Ca}^{2+}$  release. The smaller subspace volume (dotted line) produces greater  $\text{Ca}^{2+}$  release at high voltage because the small amount of trigger is more effective. However, overall gain is lower because RyR adaptation is increased. (B) The average  $[\text{Ca}^{2+}]_{\text{ss}}$  transients at  $0$  mV show that subspace volume effects both the magnitude and temporal profile of RyR  $\text{Ca}^{2+}$  release. Halving the subspace (dotted line) produces elevated sustained  $\text{Ca}^{2+}$  release during the voltage pulse ( $0.1$  to  $0.3$  s) and a small amount regenerative RyR  $\text{Ca}^{2+}$  release after the pulse when DHPR influx has ceased. Note that doubling the subspace increased peak flux at  $0$  mV (A), but produced a smaller change in  $[\text{Ca}^{2+}]_{\text{ss}}$  given the larger volume. (C) Doubling the transfer rate out of the subspace ( $\tau_{\text{xfer}}$ ) results decreases RyR  $\text{Ca}^{2+}$  release at high depolarizations (dotted line). Decreasing  $\tau_{\text{xfer}}$  by half increases the gain of RyR  $\text{Ca}^{2+}$  at higher voltages. (D) The average  $[\text{Ca}^{2+}]_{\text{ss}}$  transients at  $0$  mV show a higher peak value when  $\tau_{\text{xfer}}$  is decreased (dashed line) and a lower peak value when  $\tau_{\text{xfer}}$  is increased (dotted line).

voltages (Fig. 11 B, dotted line), and the depletion of  $\text{Ca}^{2+}$  from the SR is less for the smaller subspace volume (not shown).

The second method involves modification of the transfer rate out of the FRU subspace by altering the time constant  $\tau_{\text{xfer}}$  (transfer rate is inversely proportional to  $J_{\text{xfer}}$ ). When the transfer rate is doubled, the right side of the graded release curve (which is determined by the I-V relation) is shifted to the left (Fig. 11 C, dotted line). Similar to the increased subspace volume case, the doubled transfer rate decreases the effectiveness of the DHPR trigger at high voltages (Fig. 11 D, dotted line). Reducing the transfer rate by half causes the right side of the graded release curve to be shifted to the right (Fig. 11 C, dashed line). Here a small DHPR trigger is more effective at high voltages (Fig. 11 D, dashed line).

## DISCUSSION

The results demonstrate that this simplified model of functional release unit with Markov descriptions of DHPR and RyR channels produces both positive gain and gradedness when implemented as Monte Carlo simulations. The gradedness is generally robust with variation in the model pa-

rameters, and model behavior changes in reasonable and understandable ways (i.e., increases of SR load increase SR  $\text{Ca}^{2+}$  release). The model also gives some insight into the following areas: 1) the mechanism of release, 2) the role of SR  $\text{Ca}^{2+}$  depletion on termination of release, 3) the role of RyR adaptation on termination of release, and 4) possible physiological implications of geometry changes.

## Mechanism of release

The results illustrate that RyR  $\text{Ca}^{2+}$  release is most effectively triggered by DHPR  $\text{Ca}^{2+}$  influx, but can also be triggered by  $\text{Ca}^{2+}$  release from neighboring RyRs (Fig. 10). The latter effect of self-regenerating RyR  $\text{Ca}^{2+}$  release is shown to decrease with lower SR loads or higher RyR adaptation rates (Figs. 7, 8, and 10). The moderating effects of decreasing SR  $\text{Ca}^{2+}$  load and RyR adaptation work synergistically to keep SR unloading to  $\sim 50\%$ . RyR  $\text{Ca}^{2+}$  release is invariant with DHPR open time (Fig. 10 C).

The magnitude of the gain or amplification factor for CICR is similar to those measured experimentally (Wier et al., 1994). However, the shape of the gain curve produced by the model (Fig. 5, B and D) differs from that observed experimentally (Wier et al., 1994). This deficiency of the

model arises from the assumption that all RyR in the functional unit see the same  $[\text{Ca}^{2+}]_{\text{SS}}$ . If spatial gradients of  $\text{Ca}^{2+}$  were present, higher-amplitude DHPR fluxes seen at lower depolarizations would recruit more RyRs through a greater spatial spread of  $\text{Ca}^{2+}$  to nearby RyRs than would the lower-amplitude DHPR fluxes seen at higher depolarizations. This would result in increased gain at lower depolarizations.

### Depletion of SR and termination of $\text{Ca}^{2+}$ release

Previous modeling by our group that local depletion of SR  $\text{Ca}^{2+}$  may play an important role in terminating  $\text{Ca}^{2+}$  release. There are two proposed mechanisms. The first mechanism assumes the existence of two separate SR pools, the  $\text{Ca}^{2+}$  uptake pool (called network SR or NSR) and the  $\text{Ca}^{2+}$  release pool (called junctional SR or JSR). If  $\text{Ca}^{2+}$  transfer between these compartments is slow, then JSR can deplete, thus terminating RyR  $\text{Ca}^{2+}$  release (see Jafri et al., 1998). However, the two-pool SR is a hypothetical construct, and there is little experimental support for such a long time constant between  $\text{Ca}^{2+}$  uptake and release sites (Bers, 1991). A second mechanism assumes that the NSR-JSR transfer rate is large, so that the  $[\text{Ca}^{2+}]$  in each are very similar (i.e., SR is essentially one compartment). In this scheme, depletion occurs in both NSR and JSR (see Jafri et al., 1998). A problem with this mechanism is that our previous simulations using a deterministic model suggest that almost complete depletion occurs during  $\text{Ca}^{2+}$  release. In contrast, experimental evidence suggests a maximal SR depletion of only  $\sim 50\%$  (Janczewski et al., 1995; Bassani et al., 1995b).

The stochastic simulations here suggest that  $\text{Ca}^{2+}$  release termination can be achieved with a degree of total JSR unloading similar to that measured experimentally. In this model, the JSR is refilled by the NSR that has a fixed  $[\text{Ca}^{2+}]$ . This is clearly a simplification; however, such a construction makes it clear that SR  $\text{Ca}^{2+}$  release can terminate in the absence of a large degree of total SR  $\text{Ca}^{2+}$  depletion in SR. Indeed,  $\text{Ca}^{2+}$  release is terminated in our model despite there being a continual refilling of JSR.

The mechanism of model  $\text{Ca}^{2+}$  release termination is the loss of self-regenerating  $\text{Ca}^{2+}$  release by the RyR as the local SR empties. In the numerical experiments where a single RyR is assumed to open, a large value of  $[\text{Ca}]_{\text{JSR}}$  produced a high degree of coupling between RyR openings and a correspondingly large  $\text{Ca}^{2+}$  release (Fig. 10, *B* and *D*). In contrast, when  $[\text{Ca}]_{\text{JSR}}$  is reduced to  $400 \mu\text{M}$ , SR  $\text{Ca}^{2+}$  release is substantially diminished (Fig. 10 *D*). Hence the likelihood of self-regenerating RyR openings decreases as SR empties.

Without regeneration, the SR  $\text{Ca}^{2+}$  release can more closely follow DHPR openings, i.e., SR  $\text{Ca}^{2+}$  release occurs with DHPR openings and ceases shortly afterward. DHPR influx drives SR  $\text{Ca}^{2+}$  release for the complete duration of a voltage pulse, even after SR has depleted (i.e., see Fig. 4

*B*). From the single DHPR opening data, the SR  $\text{Ca}^{2+}$  release is approximately proportional to the SR load (Fig. 10 *C*). Therefore, at low SR loads, DHPR influx can effectively drive RyR  $\text{Ca}^{2+}$  release.

### Role of adaptation and the termination of release

A proposed role for adaptation in the cardiac myocyte is to provide negative feedback to SR  $\text{Ca}^{2+}$  release to counter the strong positive feedback of CICR (Valdivia et al., 1995). We found that modifying adaptation rate did effect the magnitude of the  $\text{Ca}^{2+}$  release event, the temporal features of the  $\text{Ca}^{2+}$  transient, and the degree of unloading of SR (Fig. 7 *B*). However, at high SR  $\text{Ca}^{2+}$  load, release is sustained as a result of regenerative RyR opening despite the presence of adaptation (Fig. 8 *B*). Moreover, even if the adaptation rate is increased 10-fold, release does not terminate in the case of high SR  $\text{Ca}^{2+}$  load (data not shown). In fact, experiments show that under the conditions of high SR  $\text{Ca}^{2+}$  load, the mean open time of the RyR increases to as high as 17.4 ms (Lukyanenko et al., 1996). They attribute this to modulation of RyR inactivation by SR  $[\text{Ca}^{2+}]$ . In the simulations, doubling SR  $[\text{Ca}^{2+}]$  increases the number of channel openings (from 14,520 to 29,490 for 500 runs) and the mean open time increases (from  $\sim 2.8$  ms to  $\sim 7.1$  ms) without the inclusion of any explicit effects of SR lumenal  $[\text{Ca}^{2+}]$  on the RyR adaptation or inactivation. The mechanism is due to the differences in  $[\text{Ca}^{2+}]$  at the mouth of the channel acting on the RyR and not on lumenal SR  $\text{Ca}^{2+}$  acting on RyR as observed by Xu and Meissner (1998). Hence, we can conclude that SR emptying plays a more crucial role in terminating  $\text{Ca}^{2+}$  release than does adaptation. We note that others stochastic modeling of diadic SR release also suggest an important role of SR depletion in the termination of release (Stern, 1992).

Adaptation may also play other important roles in shaping RyR  $\text{Ca}^{2+}$  release. The data of Fig. 10 *B* show that integrated RyR flux is essentially independent of the duration of the DHPR open time. This lack of dependence is a consequence of RyR adaptation (the RyR moving from state  $P_{O4}$  to state  $P_{C5}$ ) so that longer duration triggers do not produce additional RyR  $\text{Ca}^{2+}$ . This behavior is consistent with experimental findings that  $\text{Ca}^{2+}$  spark amplitudes are independent of the duration of the DHPR trigger current (Sham et al., 1998; Cannell et al., 1995) (see further discussion of  $\text{Ca}^{2+}$  sparks below). Other potential roles for adaptation could be to prevent secondary SR  $\text{Ca}^{2+}$  release events from occurring during an AP. Secondary SR  $\text{Ca}^{2+}$  release events are one potential mechanism for early after-depolarizations, a proarrhythmogenic condition thought to be the basis of torsades de pointe and ectopic beating (Volders et al., 1997). Our previous work also suggests that the slow recovery from adaptation may play a crucial role in shaping mechanical restitution and other interval-force relations (Rice et al., 1998, 1999). More recently, it has been shown that mechanical restitution results from slow recov-

ery of RyRs from the refractory state (Sham et al., 1999), a mechanism that has been suspected for quite some time (Bers, 1991).

### Relationship to $\text{Ca}^{2+}$ sparks

Although not the primary focus of this paper, these simulations do bear on issues regarding properties of  $\text{Ca}^{2+}$  sparks. Because our simulations do not consider the spatial aspects of the functional unit, we cannot compare our results directly to experimental spark data. However, the magnitudes and temporal aspects of unitary  $\text{Ca}^{2+}$  release can be compared to experimental data.

The simulations that most closely match  $\text{Ca}^{2+}$  sparks are the RyR  $\text{Ca}^{2+}$  release events that are triggered by a single channel opening (Fig. 10). The size and shape of the  $[\text{Ca}^{2+}]$  transients are similar to those reported in the literature (Sham et al., 1998). The half-time of decay for spark is measured to be 10 to 40 ms (Santana et al., 1996). Similar to experimental data (Sham et al., 1998; Cannell et al., 1995), we find that  $\text{Ca}^{2+}$  spark amplitudes are independent of the duration of the DHPR trigger current, and the termination of SR  $\text{Ca}^{2+}$  releases does not depend on cessation of DHPR influx. The model is also consistent with the experimental observation that  $\text{Ca}^{2+}$  spark amplitudes are correlated with SR  $\text{Ca}^{2+}$  load (Satoh et al., 1997).

In our voltage pulse simulations, the initial  $\text{Ca}^{2+}$  release events from SR are large-amplitude, and thus are more likely the summation of multiple sparks. While the larger initial  $\text{Ca}^{2+}$  release appears to be regenerative, RyR  $\text{Ca}^{2+}$  release stops in response to the termination of DHPR current when the voltage step repolarizes (under default conditions). This is consistent with findings that halting DHPR currents can stop SR  $\text{Ca}^{2+}$  release (Wier et al., 1994; Cleemann and Morad, 1991).

### Physiological implications of geometry changes

In experiments, Gomez and co-workers observed that congestive heart failure decreases coupling between trigger DHPR  $\text{Ca}^{2+}$  influx and RyR  $\text{Ca}^{2+}$  release, possibly as a result of altered geometry in diadic space. (Gomez et al., 1997). Their results showed a bell-shaped curve with decreased gain across the voltage range tested. Similar results were not obtained in our simulations of altered diadic space geometry by either of two methods, increasing FRU subspace volume or increasing the efflux rate of  $\text{Ca}^{2+}$  out of the FRU subspace. In both cases, the RyR release was decreased at high voltages, consistent with the experimental finding, but the RyR release was increased at lower voltages, an effect not observed experimentally. Because neither of these two manipulations, either individually or together, reproduces the experimental data, the simulation results suggest that other changes besides these simple geometric alterations may be needed to account for the decreased gain observed in CHF. Indeed, the simulation

results most similar to the experimental finds are for increased adaptation rate (Fig. 7, *dashed trace*) or for decreased SR load (Fig. 8, *dotted trace*). Eisner and co-workers (1998) suggest that altering either the trigger flux from DHPR or the RyR flux alone will only have transient effects on SR  $\text{Ca}^{2+}$  release and that the only net result of reduced coupling would be a decrease in SR  $\text{Ca}^{2+}$  load. In fact, a decreased SR  $\text{Ca}^{2+}$  load is observed during heart failure, due to both down-regulation of the SERCA2a pump and up-regulation of  $\text{Na}^+/\text{Ca}^{2+}$  exchange (O'Rourke et al., 1999; Winslow et al., 1999). However, Gomez and co-workers used a pulse protocol designed to control SR  $\text{Ca}^{2+}$  load in the experiments. CHF-induced changes in adaptation rate were not tested experimentally, and hence could be a potential mechanism of altered DHPR-RyR coupling during CHF.

### Other potential mechanisms of graded $\text{Ca}^{2+}$ release

While the model produces robust graded  $\text{Ca}^{2+}$  release, we cannot rule out other potential mechanisms that might also contribute to graded  $\text{Ca}^{2+}$  release in real cells. For example,  $\text{Ca}^{2+}$  diffusion in the diadic space might result in the recruitment of additional RyR in response to larger DHPR trigger  $\text{Ca}^{2+}$  influx. This mechanism could be termed recruitment within a functional unit as a result of local  $[\text{Ca}^{2+}]$  gradients in microscopic domain. Another type of recruitment could also occur if cross-coupling exists between functional units. For example, a large  $\text{Ca}^{2+}$  release in one functional unit could potentially raise the  $[\text{Ca}^{2+}]$  gradient high enough to produce  $\text{Ca}^{2+}$  release in a neighboring functional unit. There is some experimental evidence that  $\text{Ca}^{2+}$  release sites can be coherent over distances of 600 nm that are larger than an FRU (Parker et al., 1996).

While we do assume a uniform  $[\text{Ca}^{2+}]$  in each subspace, the need to consider each individual space is clear. The failure of the deterministic simulations here and elsewhere to produce graded  $\text{Ca}^{2+}$  release illustrates this point. This finding is predicted by previous work by Stern suggesting that "common pool" models, like our deterministic model, cannot produce both high gain and graded  $\text{Ca}^{2+}$  release without unrealistically tight control over parameters. In contrast, a "local control" model, like our stochastic model, can potentially reproduce graded  $\text{Ca}^{2+}$  release. Our results differ from previous work in that we show that robust high gain and graded  $\text{Ca}^{2+}$  release can occur in a model with detailed descriptions of DHPR and RyRs. Hence, these descriptions may be sufficient to explain graded  $\text{Ca}^{2+}$  release, although we cannot rule out other possible effects such as  $[\text{Ca}^{2+}]$  gradients within a functional unit or cross-coupling between functional units.

### CONCLUSIONS

A model is developed to describe the CICR in rat cardiac muscle. Using stochastic methods, CICR shows both high



gain and gradedness similar to the experimental studies. The high gain and gradedness are generally robust when parameters are varied, although the amplitude and temporal details of  $\text{Ca}^{2+}$  release do change. The model suggest that DHPR influx produces a short, high-amplitude change in subspace  $[\text{Ca}^{2+}]$  that is very effective in opening RyRs. For a single DHPR opening, the resulting RyR  $\text{Ca}^{2+}$  release flux is insensitive to the DHPR open duration but is strongly correlated with SR  $\text{Ca}^{2+}$  load, consistent with experimental  $\text{Ca}^{2+}$  spark data. In contrast, the single RyR openings require a long open duration and large SR load to be effective in triggering opening of neighboring RyRs. This low coupling between adjacent RyRs, especially as SR depletes, may explain why CICR does self-regenerate until the SR empties. Our results suggest that adaptation alone does not terminate  $\text{Ca}^{2+}$  release, but that adaptation plays an important modulatory role in shaping  $\text{Ca}^{2+}$  release duration and magnitude.

In contrast to the results above for stochastic simulations, our previous deterministic simulations show regenerative  $\text{Ca}^{2+}$  release only at optimum voltages for trigger influx (near 0 mV), but no  $\text{Ca}^{2+}$  release outside this range (i.e., all-or-none response). The failure of our deterministic model suggests that CICR cannot be predicted by assuming a single subspace to represent the ensemble average of such spaces ("common pool model"). However, our stochastic results show that robust high gain and graded  $\text{Ca}^{2+}$  release are produced when the local  $[\text{Ca}^{2+}]$  in each subspace is considered. Hence, our modeling results suggest that gradedness can occur by the recruitment of the independent functional units. Moreover, this gradedness occurs in the absence of spatial  $[\text{Ca}^{2+}]$  gradients across the functional unit or cross-coupling between functional units, although our modeling cannot rule out these other potential mechanisms.

## REFERENCES

- Bassani, J. W., W. Yuan, and D. M. Bers. 1995. Fractional SR Ca release is regulated by trigger Ca and SR Ca content in cardiac myocytes. *Am. J. Physiol.* 268:C1313–C1329.
- Bers, D. M. 1991. Excitation-contraction coupling and cardiac contractile force. Kluwer, Boston.
- Bers, D. M., and V. M. Stiffel. 1993. Ratio of ryanodine to dihydropyridine receptors in cardiac and skeletal muscle. *Am. J. Physiol.* 264:C1587–C1593.
- Beuckelmann, D. J., and W. G. Wier. 1988. Mechanism of release of calcium from sarcoplasmic reticulum of guinea-pig cardiac cells. *J. Physiol. (Lond.)* 405:233–235.
- Callewaert, G. 1992. Excitation-contraction coupling in mammalian heart cells. *Cardiovasc. Res.* 26:923–932.
- Cannell, M. B., H. Cheng, and W. J. Lederer. 1994. Spatial-non-uniformities in  $[\text{Ca}^{2+}]$  during excitation-contraction coupling in cardiac myocytes. *Biophys. J.* 67:1942–1956.
- Cannell, M. B., H. Cheng, and W. J. Lederer. 1995. The control of calcium release in heart muscle. *Science*. 268:1045–1049.
- Cheng, H., W. J. Lederer, and M. B. Cannell. 1993. Calcium sparks: elementary events underlying excitation-contraction coupling in heart muscle. *Science*. 262:740–744.
- Cheng, H., W. J. Lederer, and M. B. Cannell. 1996. Calcium sparks and  $[\text{Ca}^{2+}]$  waves in cardiac myocytes. *Am. J. Physiol.* 270:C148–C159.
- Cleemann, L., and M. Morad. 1991. Role of  $\text{Ca}^{2+}$  channel in cardiac excitation-contraction coupling in the rat: evidence from  $\text{Ca}^{2+}$  transients and contraction. *J. Physiol.* 432:283–312.
- Eager, K. R., and A. F. Dulhunty. 1998. Activation of the cardiac ryanodine receptor by sulfhydryl oxidation is modified by  $\text{Mg}^{2+}$  and ATP. *J. Membr. Biol.* 163:9–18.
- Eisner, D. A., A. W. Trafford, M. E. Diaz, C. L. Overend, and S. C. O'Neill. 1998. The control of Ca release from the cardiac sarcoplasmic reticulum: regulation versus autoregulation. *Cardiovasc. Res.* 38:589–604.
- Fabiato, A. 1985a. Simulated calcium current can both cause calcium loading in and trigger calcium release from the sarcoplasmic reticulum of a skinned cardiac Purkinje cell. *J. Gen. Physiol.* 85:291–320.
- Fabiato, A. 1985b. Time and calcium dependence of activation and inactivation of calcium-induced release of calcium from the sarcoplasmic reticulum of a skinned canine cardiac Purkinje cell. *J. Gen. Physiol.* 85:247–290.
- Gomez, A., H. H. Valdivia, H. Cheng, M. R. Lederer, L. F. Santana, M. B. Cannell, S. A. McCune, R. A. Altschuld, and W. J. Lederer. 1997. Defective excitation-contraction coupling in experimental heart cardiac hypertrophy and heart failure. *Science*. 276:800–806.
- Györke, S., and M. Fill. 1993. Ryanodine receptor adaptation: control mechanism of  $\text{Ca}^{2+}$  induced  $\text{Ca}^{2+}$  release in heart. *Science*. 260:807–809.
- Isenberg, G. 1995. Cardiac excitation-contraction coupling: from global to microscopic models. In *Physiology and Pathophysiology of the Heart*. N. Sperelakis, editor. Kluwer Academic Publishers, Boston.
- Jafri, M. S., J. J. Rice, and R. L. Winslow. 1998. Cardiac  $\text{Ca}^{2+}$  dynamics: the roles of ryanodine receptor adaptation and sarcoplasmic reticulum load. *Biophys. J.* 1149–1168.
- Janczewski, A. M., H. A. Spurgeon, M. D. Stern, and E. D. Lakatta. 1995. Effects of sarcoplasmic  $\text{Ca}^{2+}$  load on the gain function of  $\text{Ca}^{2+}$  release by  $\text{Ca}^{2+}$  current in cardiac cells. *Am. J. Physiol.* 268:H916–H920.
- Keizer, J. 1987. Statistical Thermodynamics of Nonequilibrium Processes. Springer-Verlag, New York.
- Keizer, J., and L. Levine. 1996. Ryanodine receptor adaptation and CICR-dependent  $\text{Ca}^{2+}$  oscillations. *Biophys. J.* 71:3477–3487.
- Keizer, J., and G. D. Smith. 1998. Spark-to-wave transitions: saltatory transmission of calcium wave in cardiac myocytes. *Biophys. Chem.* 72:87–100.
- Langer, G. A., and A. Peskoff. 1996. Calcium concentration and movement in the diadic cleft space of the cardiac ventricular cell. *Biophys. J.* 70:1169–1182.
- Lipp, P., and E. Niggli. 1994. Modulation of  $\text{Ca}^{2+}$  release in cultured neonatal rat cardiac myocytes: insights from subcellular release patterns in revealed by confocal microscopy. *Circ. Res.* 74:979–990.
- Lopez-Lopez, J. R., P. S. Shacklock, P. S. Balke, and W. G. Wier. 1995. Local calcium transients triggered by single L-type calcium channels in cardiac cells. *Science*. 268:1042–1045.
- Lukyanenko, V., I. Gyorke, and S. Gyorke. 1996. Regulation of calcium release by calcium inside the sarcoplasmic reticulum in ventricular myocytes. *Pflugers Arch.* 432:1047–1054.
- Luo, C. H., and Y. Rudy. 1994. A dynamic model of the cardiac ventricular action potential. I. Simulations of ionic currents and concentration changes. *Circ. Res.* 74:1071–1096.
- O'Rourke, B., D. A. Kass, G. F. Tomaselli, S. Kaab, R. Tunin, and E. Marban. 1999. Mechanisms of altered excitation-contraction coupling in canine tachycardia-induced heart failure. I. Experimental studies. *Circ. Res.* 84:562–570.
- Parker, I., W. J. Zang, and W. G. Wier. 1996.  $\text{Ca}^{2+}$  sparks involving multiple release sites along Z-lines in rat heart cells. *J. Physiol.* 497:31–38.
- Rice, J. J., M. S. Jafri, and R. L. Winslow. 1998. Modeling interval-force relations in cardiac muscle. *Biophys. J.* 74:57a. (Abstr.).
- Rice, J. J., M. S. Jafri, and R. L. Winslow. 1999. Modeling short-term interval-force relations in cardiac muscle. *Am. J. Physiol.* In press.
- Rose, W. C., C. W. Balke, W. G. Wier, and E. Marban. 1992. Macroscopic and unitary properties of physiological ion flux through L-type  $\text{Ca}^{2+}$  channels in guinea-pig heart cells. *J. Physiol. (Lond.)* 456:267–284.

- Santana, L. F., H. Cheng, A. M. Gomez, M. B. Cannell, and W. J. Lederer. 1996. Relation between the sarcolemmal  $\text{Ca}^{2+}$  current and  $\text{Ca}^{2+}$  sparks and local control theories for cardiac excitation-contraction coupling. *Circ. Res.* 78:166–171.
- Sato, H., L. A. Blatter, and D. M. Bers. 1997. Effects of  $[\text{Ca}]_i$ ,  $\text{Ca}^{2+}$  load and rest on  $\text{Ca}^{2+}$  spark frequency in ventricular myocytes. *Am. J. Physiol.* 272:H657–H668.
- Sham, J. S. K., L. Song, Y. Chen, L. Deng, M. D. Stern, E. G. Lakatta, and H. Cheng. 1998. Termination of  $\text{Ca}^{2+}$  release by a local inactivation of ryanodine receptors in cardiac myocytes. *Proc. Natl. Acad. Sci. USA.* 95:15096–15101.
- Sham, J. S. K., L. Song, M. D. Stern, E. G. Lakatta, and H. Cheng. 1999. Inactivation of cardiac ryanodine receptor (RyR): evidence from restitution of  $\text{Ca}^{2+}$  release. *Biophys. J.* 76:385a. (Abstr.).
- Smith, G. D., J. Keizer, M. D. Stern, W. J. Lederer, and H. Cheng. 1998. A simple numerical model of calcium spark formation and detection in cardiac myocytes. *Biophys. J.* 75:15–32.
- Soeller, C., and M. B. Cannell. 1997. Numerical simulations of local calcium movements during L-type channel gating in the cardiac diad. *Biophys. J.* 73:87–111.
- Stern, M. D. 1992. Theory of excitation-contraction coupling in cardiac muscle. *Biophys. J.* 63:497–517.
- Valdivia, H. H., J. H. Kaplan, G. C. R. Ellis-Davies, and W. J. Lederer. 1995. Rapid adaption of cardiac ryanodine receptor: modulation by  $\text{Mg}^{2+}$  and phosphorylation. *Science.* 267:1997–1999.
- Volders, P. G. A., A. Kulesár, M. A. Vos, K. R. Sipido, H. J. J. Wellens, R. Lazarra, and B. Szabo. 1997. Similarities between early and delayed afterdepolarizations induced by isoproterenol in canine ventricular myocytes. *Cardiovasc. Res.* 34:348–359.
- Wagner, J. M., and J. Keizer. 1994. Effects of rapid buffers on  $\text{Ca}^{2+}$  diffusion and  $\text{Ca}^{2+}$  oscillations. *Biophys. J.* 67:447–456.
- Wier, W. G., T. M. Egan, J. R. Lopez-Lopez, and C. W. Balke. 1994. Local control of excitation-contraction coupling in rat heart cells. *J. Physiol.* 474:463–471.
- Winslow, R. L., J. R. Rice, M. S. Jafri, E. Marban, and B. O'Rourke. 1999. Mechanisms of altered excitation-contraction coupling in canine tachycardia-induced heart failure. II. Model studies. *Circ. Res.* 84:571–586.
- Xu, L., and G. Meissner. 1998. Regulation of cardiac muscle  $\text{Ca}^{2+}$  release channel by sarcoplasmic reticulum lumenal  $\text{Ca}^{2+}$ . *Biophys. J.* 75:2302–2312.